

# Design of the Enzyme–Carrier Interface to Overcome the O<sub>2</sub> and NADH Mass Transfer Limitations of an Immobilized Flavin Oxidase

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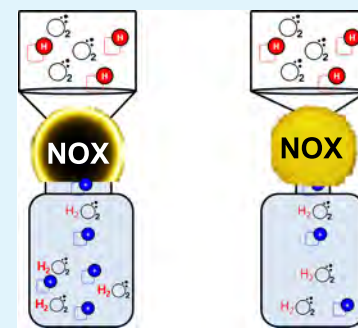


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**ABSTRACT:** Understanding how the immobilization of enzymes on solid carriers affects their performance is paramount for the design of highly efficient heterogeneous biocatalysts. An efficient supply of substrates onto the solid phase is one of the main challenges to maximize the activity of the immobilized enzymes. Herein, we apply advanced single-particle analysis to decipher the optimal design of an immobilized NADH oxidase (NOX) whose activity depends both on O<sub>2</sub> and NADH concentrations. Carrier physicochemical properties and its functionality along with the enzyme distribution across the carrier were implemented as design variables to study the effects of the intraparticle concentration of substrates (O<sub>2</sub> and NADH) on the activity. Intraparticle O<sub>2</sub>-sensing analysis revealed the superior performance of the enzyme immobilized at the outer surface in terms of effective supply of O<sub>2</sub>. Furthermore, the co-immobilization of NADH and NOX within the tuned surface of porous microbeads increases the effective concentration of NADH in the surroundings of the enzyme. As a result, the optimal spatial organization of NOX and its confinement with NADH allow a 100% recovery of the activity of the soluble enzyme upon the immobilization process. By engineering these variables, we increase the NADH oxidation activity of the heterogeneous biocatalyst by up to 650% compared to NOX immobilized under suboptimal conditions. In conclusion, this work highlights the rational design and engineering of the enzyme–carrier interface to maximize the efficiency of heterogeneous biocatalysts.



*The enzyme location matters...*

**KEYWORDS:** immobilized enzymes, substrate diffusion, O<sub>2</sub> sensing, mass transfer limitations, single-particle analysis

## INTRODUCTION

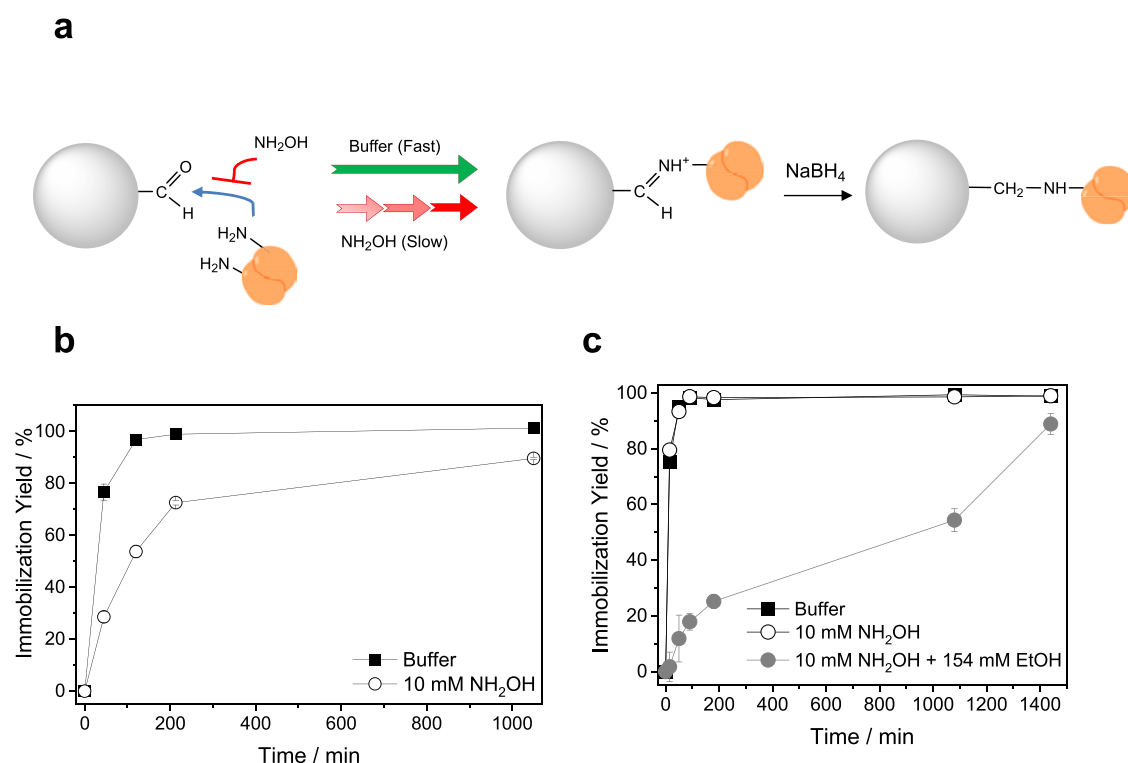
Enzyme immobilization is a key enabling technology in synthetic, analytical, and environmental chemistry. The binding of enzymes to solid materials eases the reaction control and sometimes stabilizes the resulting heterogeneous biocatalyst. Such stabilization allows the continuous and discontinuous utilization of enzymes for long operation times.<sup>1,2</sup> The functionality of immobilized enzymes inside a solid matrix relies on spatiotemporal phenomena at nano-, micro-, and macroscale.<sup>3–5</sup> For example, activity can be decreased by structural distortions and/or poor accessibility of the substrates to the enzyme active center (nanoscale), by limited substrate transport from the bulk to the material surface, which creates intraparticle gradients of the reaction components (microscale),<sup>4,6–9</sup> and by suboptimal reactor settings, like poor agitation (macroscale).

Particularly, the influence of the mass transport resistances and the resulting spatiotemporal gradients of reactants mainly depend on the carrier material characteristics (physicochemical nature and internal architecture) and the catalyst localization inside the solid matrix.<sup>10–12</sup> In heterogeneous biocatalysis, like in heterogeneous chemical catalysis, porous carriers are preferred since their higher specific area enables preparation of catalysts with high volumetric activity.<sup>13,14</sup> In porous

materials, the bound enzymes might suffer from both external mass transfer issues and internal diffusion restrictions, limiting the productivity of the heterogeneous biocatalysts. Traditionally, these mass transport issues are usually mitigated by decreasing the maximum reaction rate working at low enzyme loads (thus, sacrificing productivity), tuning carrier dimensions (particle and pore sizes) and the reactor configuration (fluid dynamics of mixing).<sup>12,14</sup> Additionally, the position of the enzymes within the carrier microstructure has also proven to be crucial to intensify the effectiveness of the heterogeneous biocatalysts<sup>15</sup> since intraparticle enzyme distribution affects how substrate mass transfer impacts the overall catalytic rate. For example, glycosidases and acylases nonuniformly immobilized at the outer surface of porous microbeads overpower those uniformly distributed across the inner material porous surface.<sup>16–22</sup>

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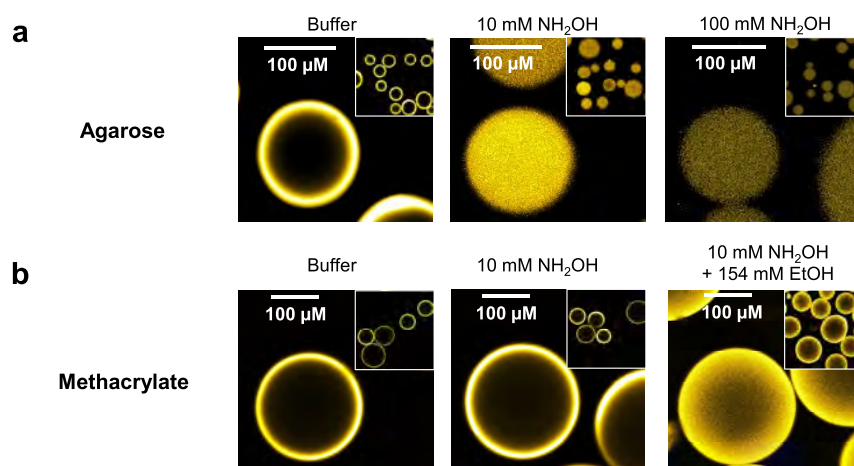
**Figure 1.** (a) Scheme of the NOX immobilization on carriers activated with aldehyde groups. NOX immobilization kinetics using (b) AG-G and (c) PU-G as porous carriers under different conditions. Enzyme load: 1 mg/g. Immobilization buffer: 100 mM sodium bicarbonate at pH 10.05.

In the last few years, our groups have proven controlling the intraparticle protein distributions by altering the immobilization rates through tuning the chemical nature of the enzyme–carrier interface.<sup>15,23</sup> In this approach, a slow immobilization process allows enzymes to diffuse within the pores and colonize the entire 3D surface of the carriers, while rapid immobilization precludes the intraparticle diffusion of the enzyme, locating them at the outer shell of the porous particles. To exert control over the immobilization rate, the immobilization chemistry plays a fundamental role since it defines the kinetics of the enzyme–carrier interactions. In previous studies, we found that the type and the density of reactive groups as well as the immobilization conditions (temperature, pH, inhibitors, etc.) determine the immobilization rate and thus the position of the enzymes across the microstructure of the carriers. Although enzyme localization may be inferred from indirect studies that measure the catalytic activity in bulk experiments,<sup>19</sup> the use of specific dyes and advances in fluorescence-based microscopy have enabled researchers to unambiguously reveal the enzyme spatial distribution and correlate it with their intraparticle specific performance through luminophores sensitive to the reaction conditions (pH, oxygen, redox environment, etc.).<sup>24</sup>

There are multiple examples where mass transfer effects are critical for catalyst efficiency. For instance, the process implementation of NAD(P)H flavin oxidases (NOX) poses some difficulties. This family of enzymes is often exploited as cofactor recycling partners in NAD<sup>+</sup>-dependent oxidation reactions, where substrate concentrations are rather low due to the poor water solubility of the oxygen and process-imposed substoichiometric amounts of the nicotinamide cofactors.<sup>25,26</sup> Moreover, NOX especially requires exogenous FAD as a redox mediator<sup>27</sup> and O<sub>2</sub> as an electron acceptor to oxidize NADH to NAD<sup>+</sup>, producing H<sub>2</sub>O<sub>2</sub> as a side product and

consequently *in situ* recycling the pool of the oxidized cofactor. Otherwise, the oxidase activity is too low for practical purposes. In this scenario, the low concentration of oxygen, NADH, and FAD limits the NOX activity,<sup>28–31</sup> an issue that turns out to be dramatic when enzymes are immobilized on porous materials as these substrates and redox mediators must diffuse from the bulk (liquid) to the biocatalyst (solid phase). The intraparticle O<sub>2</sub> depletion has been identified as one of the bottlenecks to intensify biotransformations driven by oxidases.<sup>32–35</sup> On the other hand, increasing the substrate concentration is not an option for high-cost molecules like NADH, in order to guarantee the process economics. While O<sub>2</sub> and NADH limitations could be alleviated by application of the traditional approaches mentioned above, the engineering of the spatial distribution of the immobilized enzymes and their confinement with their limiting substrates (NADH) and redox mediators (FAD) are approaches never intended before to mitigate the diffusion restrictions underlying these enzymes.

In this work, we aim at designing an immobilized NOX from *Thermus thermophilus* HB27,<sup>36</sup> through an integrative manner that involves the control of the enzyme localization, the tuning of material's physicochemical properties, and the use of advanced internal sensing to ultimately mitigate the diffusion restrictions underlying this enzyme. To that end, we have prepared a battery of heterogeneous biocatalysts with different enzyme spatial organizations within different porous materials and further tested them under different mixing conditions. Evaluating all these influential parameters, we enhance by 6.5-fold the catalytic performance of the best heterogeneous biocatalyst, reaching an immobilization effectiveness close to one, which means that its specific activity was close to the one reported for the free enzyme.



**Figure 2.** Spatial distribution of NOX immobilized on (a) agarose (AG-G) and (b) methacrylate (PU-G) microbeads under conditions described on the top of the micrographs. Autofluorescence of intrinsically FAD bound to resting NOX was harnessed to image the protein distribution. Images were analyzed using FIJI (software for image analytics). A yellow hot LUT (Lookup Table for color grading) of the fluorescence signal is depicted.

**Table 1. Immobilization Parameters of Different Preparations of NOX Immobilized on Different Carriers Activated with Glyoxyl Groups<sup>a</sup>**

carrier material	intraparticle protein distribution	protein load (mg/g carrier)	immobilization yield (%)	specific activity (U/mg)	relative recovered activity (%)
agarose (AG-G)	not uniform (outer surface)	1	100	5.66	55
	uniform	0.9	90	1.88	18
methacrylate (PU-G)	not uniform (outer surface)	1	100	2.43	24
	uniform	0.9	89	1.70	17

<sup>a</sup>Reaction conditions: air-saturated 25 mM sodium phosphate buffer pH 7.0, 25 °C, 0.15 mM FAD, and 0.2 mM NADH under orbital shaking. Specific activity of soluble NOX = 10.2 U/mg.

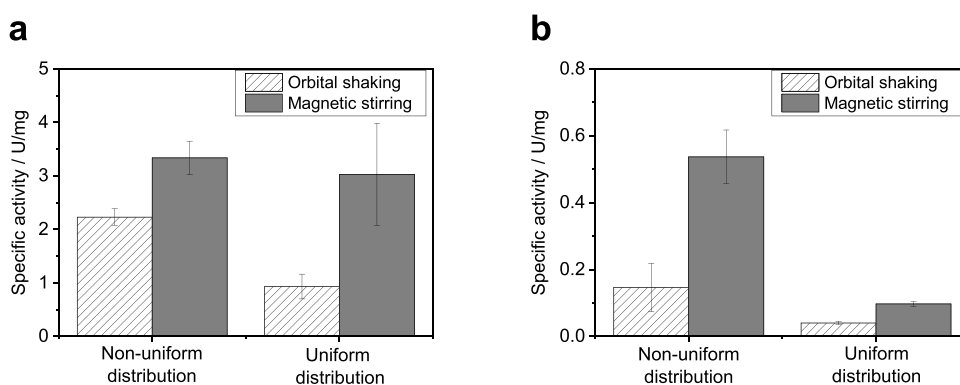
## RESULTS AND DISCUSSION

**Effect of NOX Spatial Organization on the Activity of the Immobilized Biocatalyst.** NOX was immobilized through aldehyde chemistry as previous results from our groups have proven to significantly stabilize NOX.<sup>27</sup> We used two classical carriers activated with glyoxyl (short-arm aliphatic aldehyde) groups but with different physicochemical properties. One carrier is based on hydrophilic porous 6% agarose beads (AG-G) with a particle size of 50–150 μm and average pore size of 112 nm,<sup>37</sup> while the other is based on hydrophobic porous methacrylate beads (PU-G) with both larger particle (100–300 μm) and average pore (150 nm) sizes than the agarose ones. Using both carriers, NOX was quantitatively immobilized in 30 min under alkaline conditions driven by the nucleophilic attack of the ε-NH<sub>2</sub> groups of Lys in the NOX surface, to the aldehydes of the carrier (Figure 1). These reactions formed reversible imines that were further reduced to the corresponding amine groups to make the enzyme attachment irreversible (Figure 1a). SDS-PAGE analysis reveals that the enzyme was irreversibly attached to the carrier as no protein was detected after incubating the immobilized enzymes under denaturing conditions (Figure S1).

Confocal laser scanning microscopy (CLSM) studies confirmed that NOX was mainly immobilized at the outer surface of both types of porous particles, according to previous results (Figure 2).<sup>18,19,21–23</sup> To study the effect of the spatial distribution on the performance of immobilized NOX, we immobilized this enzyme in the presence of small molecules acting as immobilization competitors. According to this, Figure 1b shows how the presence of hydroxylamine (NH<sub>2</sub>OH)

reduces the immobilization rate of NOX on AG-G. The lower immobilization rate resulted in a supported biocatalyst where NOX was uniformly distributed across the porous surface of the carrier (Figure 2a). NH<sub>2</sub>OH is highly reactive with aldehydes and thus slows down the immobilization through competing with the Lys residues of NOX. The use of immobilization competitors was previously reported to control the spatial organization of His-tagged enzymes on carriers activated with metal chelates.<sup>15</sup>

Unfortunately, NH<sub>2</sub>OH by itself was unable to slow down the immobilization of NOX on PU-G (Figure 1c). Such failure was manifested in the CLSM images (Figure 2b) where the spatial distribution of NOX was the same regardless of the presence of NH<sub>2</sub>OH during the immobilization process. The hydrophobic nature of the methacrylate materials may explain the inability of immobilization competitors to control the spatial organization of NOX. While the enzyme immobilization on AG-G is mainly driven by the aldehyde chemistry, PU-G can promote unspecific hydrophobic interactions that rapidly immobilize NOX even in the presence of NH<sub>2</sub>OH. We demonstrated such unwanted hydrophobic interactions by incubating NOX with methacrylate beads lacking the aldehydes. As expected, 77% of the offered protein was bound to the carrier after 20 h. At this point, we decided to modify the immobilization media to avoid such hydrophobic interactions. To that aim, we added 30% ethanol to reduce the polarity of the media and preclude the unspecific adsorption of NOX on the acrylic carrier PU-G. Pleasantly, we observed that the combination of ethanol and NH<sub>2</sub>OH slowed down the immobilization of NOX on PU-G (Figure 1b), suggesting that



**Figure 3.** Effect of the mixing on the apparent activity of the immobilized NOX on PU-G at a loading of (a) 0.1 mg/g and (b) 3 mg/g. Reaction conditions: 0.2 mM NADH, 0.15 mM FAD at 25 °C in 25 mM sodium phosphate buffer pH 7.0.

now the immobilization was driven by the aldehyde chemistry rather than by the hydrophobic interactions. The slower immobilization promoted the infiltration of NOX to the inner surface of PU-G (Figure 2b). These results agree with previous data reported for the lipase immobilization in the presence of ethanol, which decreases the enzyme immobilization rate.<sup>38</sup> Thus, reducing the protein immobilization rate on the more hydrophobic acrylic-based carriers required two different immobilization competitors to obtain uniform protein distributions across the material microstructure. Hence, we demonstrate that the spatial organization of protein on these carriers must be controlled, targeting two different immobilization mechanisms: aldehyde covalent chemistry and hydrophobic adsorption.

The activity of the immobilized NOX with different spatial distributions was assessed by a standard colorimetric assay where an air-saturated buffer and low concentration of NADH were used. The spatial distribution of NOX across porous carriers affected enzyme-recovered activity upon the immobilization process (Table 1). The specific activity of immobilized NOX ranged 17–55% of its soluble counterpart, depending on the material type and the enzyme spatial organization. When NOX is located at the outer surface of agarose and acrylic materials, the resulting heterogeneous biocatalysts were 3 and 1.4 times more active, respectively, than when the enzyme was uniformly distributed toward them. Table 1 also shows that NOX nonuniformly immobilized on agarose carriers outperforms the same enzyme immobilized on the acrylic ones. A plausible explanation for such a difference is that the hydrophilic nature of the agarose beads may either prevent negative structural enzyme rearrangements or benefit the mass transport of the substrates,<sup>10–12</sup> compared to the more hydrophobic methacrylate resin.

We hypothesize that the differences found in specific activity for the two enzyme distributions might be explained by a different level of the substrate restrictions toward the resulting heterogeneous biocatalyst. In order to elucidate the influence of spatial distribution on the substrate restrictions and further mitigate them by the design of the enzyme–surface interface, we performed a series of experimental analyses tuning different variables such as enzyme loading and mixing conditions.

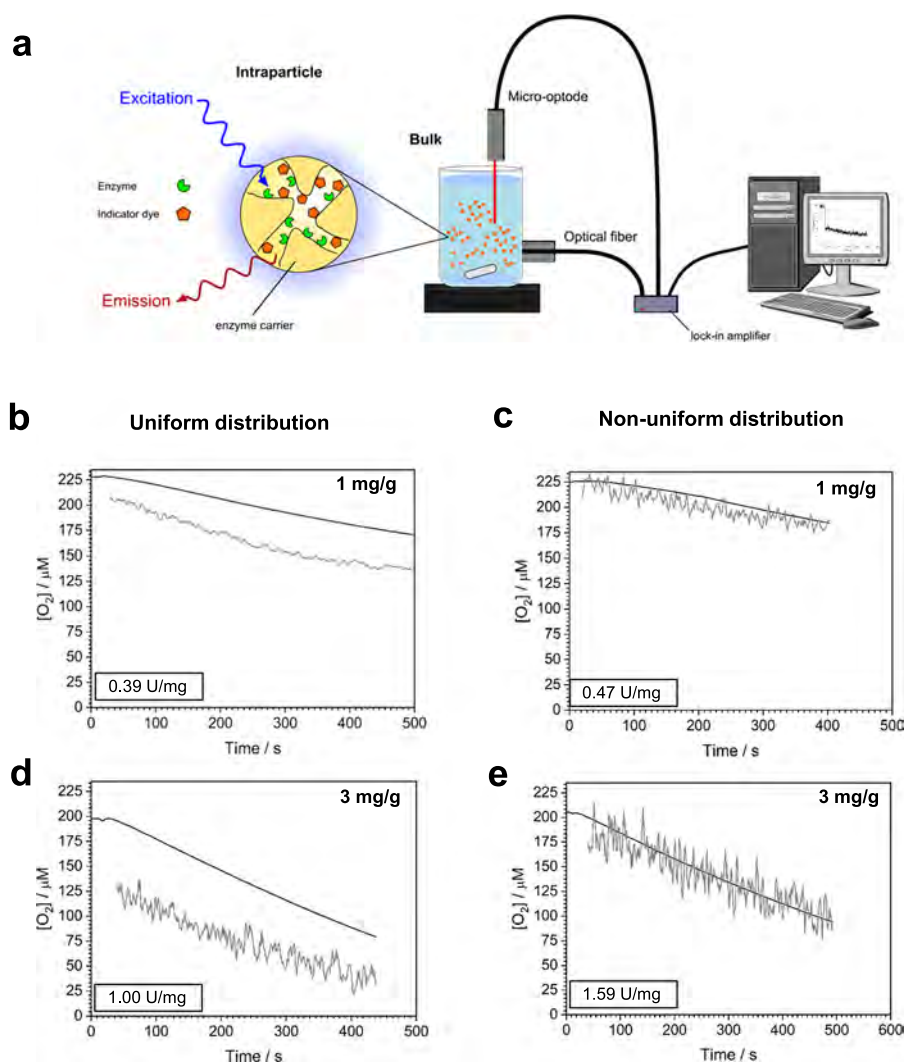
**Interrogating the Measurable Activity of Immobilized NOX with Different Spatial Organizations.** The assay conditions for immobilized NOX significantly influence the results of its measurable activity since it relies on two limiting substrates (oxygen and NADH) that need to be

transferred from the liquid and liquid/gas interphase (reaction bulk) to the solid phase (the biocatalyst). We study the enzyme activity using different biocatalysts and analysis conditions to elicit the limiting factors for the substrate mass transfer restrictions. To do so, NOX immobilized on both AG-G and PU-G with different loads and spatial distributions was measured under different mixing conditions (Figure 3 and Figure S2).

Our first observation is that the specific activity increased under magnetic stirring for all the preparations but with significant differences among the carriers and the protein spatial distributions (Figure 3 and Figure S2). Expectedly, the better mixing conditions (magnetic stirring) result in more active heterogeneous biocatalysts, which is explained by the enhancement of the external mass transfer coefficients. This effect was more noticeable in AG-G carriers where the specific activity of the immobilized enzyme under magnetic stirring was roughly 10 times larger than under orbital shaking (Figure S2). Second, we find out that the specific activity of the immobilized enzyme significantly decreases at high protein loads, but it is highly influenced by both enzyme distribution and mixing conditions. The decrease of the apparent specific activity of the immobilized enzyme upon the increase of the loading is usually reasoned as being caused by substrate mass transfer restrictions since the increase of substrate consumption rate eventually surpasses the supply rate of substrate toward the enzyme.<sup>12,20,32</sup>

For low loadings (0.1 mg/g), the effect of the spatial distribution on the NOX activity only occurred under orbital shaking where the external diffusion restrictions are more dramatic (Figure 3a). We corroborate how the uniform distributions suffer a more aggravated substrate limitation, probably due to the thicker enzyme shell (a longer diffusional distance) through which the limiting substrate must diffuse. On the contrary, when external mass transfer resistances are erased (magnetic stirring) for low loading biocatalysts, uniform and nonuniform heterogeneous biocatalysts presented similar high specific activity regardless of the enzyme spatial distribution.

For high loadings (3 mg/g), the biocatalysts were significantly less active than low-loading biocatalysts regardless of the mixing conditions and the enzyme spatial distribution (Figure 3b). A higher activity was observed under magnetic stirring conditions, but the nonuniform distribution now overpowered the uniform distribution under all the conditions. Unlike low loadings, the spatial distribution of NOX affected



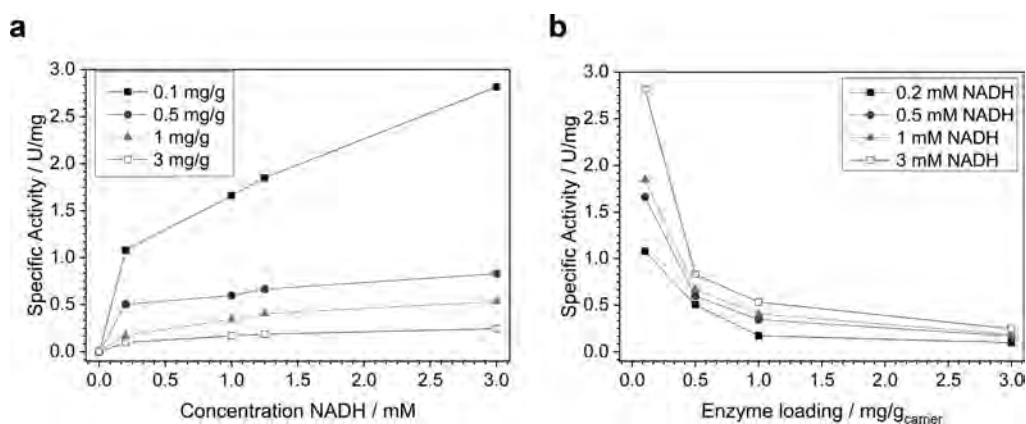
**Figure 4.** Oxygen time courses during the NADH oxidation catalyzed by different preparations of immobilized NOX. (a) Scheme of the principle of optochemical oxygen sensing in immobilized enzymes. Measurement of the space-averaged time-resolved internal  $O_2$  concentration is based on the preparation of  $O_2$ -sensitive carrier material. The reading of the internal  $O_2$  was carried out by a contactless measurement with a fiber optic integrated with a phase modulation oxygenmeter, (details can be found in the Supporting Information). The scheme was adapted with permission from ref 32. Copyright 2020 John Wiley and Sons. (b–e) Time courses of the average intraparticle oxygen concentration (gray line) and the corresponding oxygen concentration in bulk (black line) when  $O_2$  is utilized as a substrate by an immobilized NOX. Enzyme distribution, protein loading (mg/g), and measured activity (U/g) of each biocatalyst are depicted in the graphs. Measurements were performed at 37 °C, 12  $\mu\text{M}$  FAD, and 2 mM NADH.

more significantly the specific activity of NOX immobilized on PU-G under magnetic stirring than under orbital shaking. Remarkably, immobilized NOX exhibited a specific activity of 0.097 and 0.54 U/mg under magnetic stirring, when the enzyme was uniformly and nonuniformly distributed within the carrier, respectively. Therefore, the control of the protein spatial organization permits an up to 5.5 times increase in the activity of highly loaded heterogeneous biocatalysts under magnetic stirring conditions, yet the specific activity is 19 times lower than the free enzyme (10.2 U/mg).

Hence, the optimal mixing conditions and the most suitable spatial distribution were insufficient to overcome the substrates' (both oxygen and NADH) mass transport restrictions posed by the high immobilized enzyme loads. In this scenario, internal diffusional restrictions may limit the apparent activity, especially that of the uniformly distributed enzymes,<sup>32,39</sup> as described for several hydrolases.<sup>17,40</sup> To assign the magnitude of the influence of NADH and  $O_2$  limitations

and design strategies for their further mitigation, we studied the kinetics of oxygen time consumption courses provided by different NOX immobilized preparations.

**Deciphering the Influence of Oxygen Internal Diffusional Limitations and Mitigation by the Spatial Organization of the Immobilized NOX.** To identify the internal diffusional limitations of  $O_2$ , we study  $O_2$  consumption courses during the oxidation of NADH catalyzed by different preparations of immobilized NOX. To visualize the intraparticle oxygen gradient, we have monitored  $O_2$  concentration both in the liquid bulk and inside the particles following the established procedures (Figure 4a).<sup>5,33</sup> The  $O_2$  concentration in the liquid bulk was monitored using a commercial oxygen microoptode, whereas the internal  $O_2$  concentration was quantified by optochemical sensing enabled by the co-immobilization of an  $O_2$ -sensitive luminescence dye with the enzyme inside the particles. PU-G carriers were used for immobilization and further  $O_2$  sensing since this type of



**Figure 5.** Specific activity of the NOX immobilized with a nonuniform distribution at different enzyme loadings with regard to (a) the concentration of NADH and (b) the protein load. NOX immobilized on PU-G through a nonuniform distribution and operated under magnetic stirring. Reaction conditions: 0.2–3 mM NADH, 0.15 mM FAD at 25 °C in 25 mM sodium phosphate buffer pH 7.0.

material is easily functionalized with the luminesce  $O_2$  sensors through hydrophobic interactions.<sup>5</sup> Unfortunately, the hydrophilic nature of AG-G made unfeasible the integration of such luminophore within the porous structure to measure the intraparticle  $O_2$  concentration.

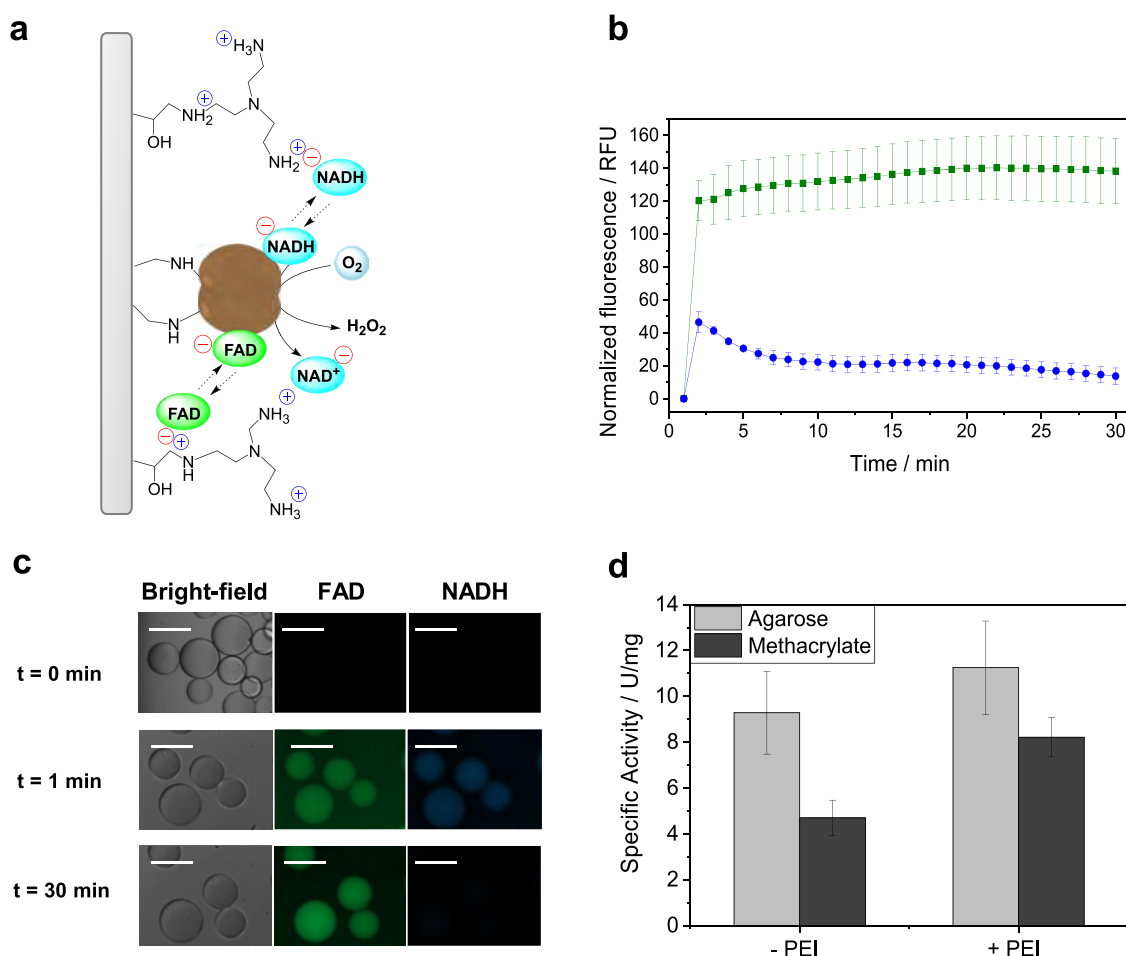
Measurements were performed for heterogeneous biocatalysts differing in enzyme distribution, enzyme loading, and using different NADH concentrations. When low-loading (0.1 mg/g) immobilized NOX was used, the time courses of internal and external oxygen were superimposable (results not shown). Hence, oxygen gradients were not detected in accordance with the high recovered activity of low-loading heterogeneous biocatalysts measured under magnetic stirring since oxygen diffusional limitations are unexpected to occur in this context.<sup>32</sup>

The same results were obtained when low concentration of NADH (<0.5 mM) was used regardless of the biocatalyst loading. To focus on the oxygen limitations, we increased the NADH concentration up to an apparent saturating concentration (2 mM). Figure 4b–e shows a set of exemplary results of the time courses of the oxygen consumption at saturating concentration of NADH using different immobilized and labeled biocatalysts. Here, we observed significant differences depending on the spatial organization of the immobilized NOX when high loads (>1 mg/g) were used. Heterogeneous biocatalysts with uniform distributions show an oxygen gradient between bulk and intraparticle conditions (Figure 4b,d), indicating that the space-averaged oxygen concentration available for the enzyme within the carrier is remarkably lower than in the bulk. On the contrary, we observed no detectable difference between the external and internal oxygen concentration when using the nonuniformly distributed heterogeneous biocatalyst, demonstrating that enzyme location enables reaching a higher local oxygen concentration (Figure 4c,e). In fact, the higher activity determined from the bulk time-course oxygen consumption corroborates these results. Measurement of the available  $O_2$  concentration inside solid carriers provided direct evidence of the occurrence of diffusional restrictions undergone by  $O_2$ -dependent immobilized enzymes.<sup>32,34,35</sup> In the literature, we find that enzyme loading and particle size critically influence the diffusional limitations and hence the measurable specific activity of the immobilized enzyme.<sup>39–41</sup> Herein, we show, for the first time, how the oxidase localization into the external shells of the particle is also a

key parameter to minimizing the oxygen gradient and therefore mitigating the limitations of the oxygen supply to the immobilized enzyme. Once we minimized the  $O_2$  internal diffusional limitations, we focus on deciphering the influence of the NADH concentration.

**Deciphering the Influence of NADH Concentration on the Performance of Immobilized NOX.** The dependency of the activity upon NADH concentration was measured in the absence of external mass transfer resistances under optimal mixing conditions for the catalysts with a nonuniform distribution. To determine the internal mass transport restrictions suffered by the immobilized NOX at different protein loads, we quantified their initial reaction rates by monitoring the oxygen consumption at different NADH concentrations. To this aim, we performed the oxidation reaction using NOX immobilized at the outer surface (nonuniform distribution) of PU-G under magnetic stirring. Figure 5 shows the specific activity of the immobilized NOX at different NADH concentrations (see also Figure S3 for the same representation in measurable activity; U/g carrier).

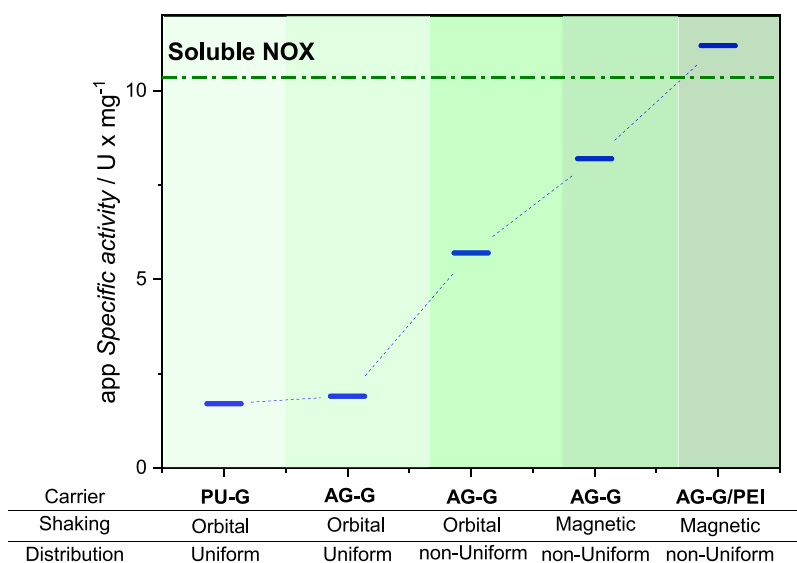
The activities of all immobilized biocatalysts increase with the NADH concentration, which indicates that all the measurements performed in standard conditions (0.2 mM NADH, air-saturated) are already dramatically limited by the cofactor available in the bulk. Especially, the specific activity of the biocatalyst with the lowest loading is significantly sensitive to the NADH concentration. At 3 mM NADH, the recovered activity of the low-loading biocatalyst reaches 30% of the activity corresponding to the free enzyme. As expected, the heterogeneous biocatalysts with higher loads displays lower specific activity under all NADH concentrations herein tested. Even at a high apparently saturating concentration of NADH and nonuniform distribution measured under optimal mixing conditions, the specific activity is still below 5% of the free enzyme. Given the high dependency of the activity on the cofactor concentration and the low specific activity detected for high enzyme loads, it is critical to implement a biocatalyst design that allows an efficient management of the cofactor transport without the need for a highly unfeasible external supply of NADH. This is especially important not only due to the precious value of the NADH but also because the NOX is conceived to serve as a cofactor-regenerating enzyme in redox biocascades, where the external concentration of NADH tends to be minimized.<sup>42</sup>



**Figure 6.** Analysis of cofactor co-immobilization. (a) Scheme of NOX (brown) and cofactors co-immobilization on AG-G coated with PEI. (b) Single-particle immobilization course of FAD (green) and NADH (blue) on AG-G immobilizing NOX and coated with PEI. (c) Epifluorescence microscopy images at different times recording bright field, the autofluorescence of both FAD (green) and NADH (blue). White scale bars correspond to 100  $\mu\text{m}$ . (d) Effect of cofactor co-immobilization on the recovered specific activity of the heterogeneous biocatalyst (1 mg/g) using two different carriers under magnetic stirring, AG-G (light gray), and PU-G (dark gray).

**Co-immobilization of NOX and NADH to Reduce the Substrate Internal Diffusion Restrictions Underlying the Heterogeneous Biocatalysts.** Suitable mixing conditions (magnetic stirring) minimize external mass transfer restriction of both oxygen and NADH, while the localization of NOX at the outermost regions of the porous carriers mitigates the internal oxygen diffusion restrictions. However, we still face some internal transport issues for the NADH, overall using more hydrophobic porous materials like PU-G. Under high NADH concentration in the bulk (3 mM), NOX nonuniformly immobilized on PU-G and AG-G with 1 mg/g load expressed a specific activity of 0.4 and 7.4 U/mg, respectively. These values mean 4% and 73% of the free enzyme specific activity (10.2 U/mg) under the same assay conditions. It is cumbersome to achieve highly active heterogeneous biocatalysts since intraparticle NADH gradients seem to jeopardize the activity of the immobilized NOX. To overcome this issue, we propose co-immobilizing NOX and NADH within the same porous particle to saturate the enzyme surroundings with its corresponding substrate and consequently minimize NADH internal gradients. To that aim, we coated immobilized NOX nonuniformly distributed with polyethyleneimine (PEI) to make a cationic layer that reversibly binds NADH through its negatively charged phosphate groups (Figure 6a). We have

recently exploited this proceeding to ionically adsorb phosphorylated cofactors in the microenvironments of cofactor-dependent enzymes.<sup>43–45</sup> Such electrostatic interactions between the cofactor and the carrier porous structure establish an association/dissociation equilibrium that allows cofactor molecules to reach the NOX active sites within the intraparticle space. Since NOX activity also demands substoichiometric amounts of flavin cofactors (FAD) as a redox mediator to transfer the electron from NADH to the oxygen,<sup>27,46</sup> we also intended to mitigate the mass transport restrictions potentially undergone by FAD. Our hypothesis is that the co-immobilization of FAD and NADH in the surrounding of the immobilized enzymes may enhance the effectiveness of the heterogeneous biocatalyst. Increasing the FAD concentration in the bulk has proven to increase the activity of soluble NOX.<sup>27</sup> Expectedly, NADH is ionically adsorbed to agarose microbeads coated with PEI with  $K_d = 46 \pm 6 \mu\text{mol g}^{-1}$  according to its Langmuir isotherm (Figure S4). In addition, we also confirmed that FAD was reversibly bound to the PEI layer. According to its Langmuir isotherm, FAD presented a  $K_d$  ( $13 \pm 1 \mu\text{mol g}^{-1}$ ) 3.5 times lower than that of NADH although both phosphorylated cofactors reached similar maximum loadings, roughly 200  $\mu\text{mol g}^{-1}$ . This means that FAD is adsorbed more strongly to the PEI layer



**Figure 7.** Engineering path to enhance the apparent specific activity of immobilized NOX. Reaction conditions for all measurements: 0.2 mM NADH, 0.15 mM FAD at 25 °C in 25 mM sodium phosphate buffer pH 7.0. The load of the immobilized enzymes was 1 mg g<sup>-1</sup> in all cases.

than NADH, but that absorption is still reversible enough for it to reach the active sites of the immobilized NOX.

Next, we studied the kinetics of the immobilization of both phosphorylated cofactors through single-particle analysis, where the ionic adsorption of both NADH and FAD were monitored by reading their autofluorescence under an epifluorescence microscope. In both cases, quantitative cofactor adsorption was accomplished in less than 1 min (Figures S5–S7), and they were uniformly distributed across the surface of the agarose microbeads, unlike NOX that was mostly located at the outer regions of the particles according to confocal laser scanning microscopy images (Figure S8). Such a uniform spatial distribution coincides with the distributions found for other phosphorylated cofactors (NADPH and PLP) immobilized on other cationic porous carriers.<sup>44,45</sup> When both NADH and FAD were mixed with the heterogeneous biocatalyst coated with PEI, we observed an extremely fast decay of the NADH autofluorescence within the porous particles (Figure 6b) as a consequence of the NADH oxidation to NAD<sup>+</sup> (lower autofluorescence) catalyzed by the immobilized NOX in the presence of FAD. The fast immobilization of NADH precluded simultaneously monitoring the complete immobilization and the reaction time course, yet the single-particle studies allowed *in operando* visualization of the confined reaction where NOX uses FAD to oxidize NADH (Figure 6c). Single-particle studies evidence that the NADH and FAD, as soon as they are in contact with the reaction mixture, are absorbed into the porous materials where NOX is immobilized and the oxidative reaction instantaneously occurs.

The cationic coating thus enables the concentration of both NADH and FAD in the surroundings of the immobilized enzymes. Figure 6d compares the recovered specific activity of NOX nonuniformly immobilized and coated with PEI at 1 mg/g protein loads on two different carriers: AG-G and PU-G under magnetic stirring. The presence of PEI increases the activity of NOX immobilized on AG-G and PU-G by 22 and 200%, respectively, since the solid phase now concentrates both NADH and FAD in the surroundings of the enzyme. The 38% lower apparent  $K_M$  values toward NADH when the immobilized NOX was coated with PEI (Figure S9) support

that the effective NADH concentration (substrate) within the porous beads is higher than in the bulk, which enhances the specific activity of the immobilized NOX. In fact, the apparent  $k_{cat}$  of NOX immobilized on AG-G increases roughly two times when coated with PEI, regardless of the protein distribution, reaching a similar value to that previously reported for the soluble enzyme.<sup>27</sup> The saturation of the NOX surroundings with NADH and FAD was remarkably beneficial when the enzyme was immobilized on PU-G since the cationic PEI layer now overcomes the NADH external diffusion restrictions posed by the hydrophobic nature of this acrylic carrier. We also studied the effect of NADH co-immobilization on the H<sub>2</sub>O<sub>2</sub> production rate that provides information about the second step of the NOX reaction where the reduced flavin transfers the electron to oxygen as the final acceptor. To this aim, we coupled an NADH-compatible colorimetric peroxidase assay to quantify both the consumed NADH and the formed H<sub>2</sub>O<sub>2</sub>. We converge into the same result: the co-immobilization of NADH and NOX on agarose carriers increases its specific activity (Figure S10).

Figure 7 summarizes all technological efforts done to increase the NOX activity along the different engineering stages. Through this optimization trip, we have ramped up the apparent specific activity value of immobilized NOX by 6.5-fold, through selecting the hydrophilic carriers like agarose, locating the enzymes at the outer surface of the microbead carriers, operating the heterogeneous biocatalyst under optimal mixing conditions (magnetic stirring), and confining both enzymes and substrates within the same carrier particle. This outstanding activity enhancement was possible through mitigating both oxygen and NADH mass transfer restrictions, giving rise to an immobilized NOX whose apparent specific activity is  $11 \pm 2$  U/mg—an effectiveness of roughly 100% compared with the free NOX measured under the same aeration, temperature, and pH conditions and using the same substrate concentrations.

## CONCLUSIONS

The optimization of heterogeneous biocatalysts based on cofactor and oxygen-dependent oxidoreductases is not trivial.



Herein, we have optimized the immobilization of NOX from a thermophilic organism on porous carriers to mitigate those substrate mass transport issues that limit the catalytic performance of an immobilized biocatalyst. We first engineered the spatial distribution of NOX across the porous surface using two different carriers based on agarose and acrylic materials. We found that the outer localization of the enzyme improves the effective supply of oxygen, enhancing the specific activity of the biocatalysts. Then, we studied the effect of the mixing conditions on the enzyme activity. The more efficient mixing conditions (provided by stirring magnetic bars) are reflected by the higher activity of the immobilized enzyme. Finally, to overcome the NADH transport limitation, we co-immobilized the enzyme with the substrate: NADH, and its redox mediator, FAD. This heterogeneous biocatalyst only needed the exogenous supply of the molecular oxygen to work; therefore, under optimal O<sub>2</sub> supply, its apparent catalytic efficiency scaled up to its maximum value. This study exemplifies the critical design and characterization aspects to control the spatiotemporal gradients occurring inside the heterogeneous biocatalysts, thus maximizing catalyst productivity. This was possible through a multiscale control of the interactions between the enzyme, the substrates, and the carriers rather than using carriers with different dimensions. Therefore, we herein deploy a set of state-of-the-art characterization techniques that merge conventional bulk steady-state experiments and intraparticle microscopic measurements to guide us during the preparation of more efficient and robust heterogeneous biocatalysts.

## EXPERIMENTAL SECTION

**Materials.** The flavine adenine dinucleotide oxidized form (FAD), hydroxylamine, ethanolamine, peroxidase from horseradish, polyethyleneimine 25 kDa (PEI25), Ampliflu Red, ampicillin, and IPTG were acquired from Sigma-Aldrich (St. Louis, IL). Nicotinamide adenine dinucleotide reduced sodium salt (NADH) was purchased from GERBU Biotechnik GmbH (Wieblingen, Germany). Plain agarose microbeads were purchased from ABT technologies (Madrid, Spain) to fabricate glyoxyl-agarose. Tris(4,7-diphenyl-1,10-phenanthroline) ruthenium (II) dichloride (Ru(dpp)<sub>3</sub>) was purchased from ABCR GmbH. Lifetech PuroLite ECR 8215F was kindly donated by PuroLite Ltd. (Llantrisant, U.K.). Inc. Eight-well microslides were supplied by Ibidi (Planegg, Germany). All other reagents and solvents were of analytical grade or superior.

**Protein Expression and Purification.** NOX was overexpressed in *E. coli* as follows.<sup>47</sup> Briefly, 1 mL of an overnight culture of *E. coli* BL21-Gold transformed with the respective plasmid (*nox*\_pET22a) was inoculated in 50 mL of LB medium containing ampicillin (100 μg/mL). The culture was incubated at 37 °C and 200 rpm until the OD<sub>600nm</sub> reached 0.6. At that point, the culture was induced with 1 mM IPTG. Cells were grown at 37 °C for 3 h and then harvested by centrifugation at 4000g for 30 min at 4 °C. The resulting pellet was resuspended in 5 mL of 25 mM sodium phosphate at pH 7. Cells were broken by sonication (LABSONIC P, Sartorius Stedim biotech) at 30% of the amplitude (5 s ON, 5 s OFF) for 30 min. The suspension was centrifuged at 10000g for 30 min at 4 °C. The supernatant was incubated at 80 °C for 45 min. The protein solution was then centrifuged at 10000g for 30 min at 4 °C to separate NOX in the supernatant. The purification process of NOX was checked by SDS-PAGE (Figure S11).

**Protein Quantification.** Bradford protein assay<sup>48</sup> was adapted to 96-well plates. Briefly, 5 μL of enzyme solution were mixed with 200 μL of Bradford reagent and incubated at room temperature for 5 min. Then, the absorbance was measured at 595 nm and the protein content was estimated employing a calibration curve using BSA as a standard.

**Enzymatic Activity Assay.** One unit of activity was defined as the amount of enzyme needed to oxidize 1 μmol of NADH at 25 °C. The decrease in the absorbance was spectrophotometrically monitored at 340 nm. Two measurement formats were employed as follows:

**Well Plate.** 200 μL of 0.15 mM FAD and 0.2–2 mM NADH in 25 mM sodium phosphate buffer at pH 7 was incubated with 10 μL of enzymatic solution or suspension in a 96-well plate under orbital shaking.

**Cuvette.** 1.5–2 mL of 0.15 mM FAD and 0.2–2 mM NADH in 25 mM sodium phosphate buffer at pH 7 was incubated with 10 μL of enzymatic solution or suspension in a cuvette under magnetic stirring.

**Activation of Supports.** Glyoxyl-agarose (AG-G) and glyoxyl-PuroLite (Pu-G) were prepared as described elsewhere.<sup>49</sup> Briefly, 1 g of either epoxy-agarose or epoxy-methacrylate was incubated with 10 mL of 100 mM H<sub>2</sub>SO<sub>4</sub> overnight and under orbital shaking. Then, the resin was filtered and washed 10 times with 10 volumes of water. To oxidize the resulting glyceryl support, 10 mL of 30 mM NaIO<sub>4</sub> was added and the suspension was incubated for 2 h under orbital shaking. Finally, the glyoxyl support was washed 10 times with 10 volumes of water and stored at 4 °C until use.

**Immobilization of NOX on Glyoxyl-Activated Carriers.** 10 mL of NOX (0.01–0.3 mg/mL) in 100 mM sodium bicarbonate buffer at pH 10 was mixed with 1 g of AG-G and incubated at room temperature under orbital shaking for 3 h. The immobilization course was followed spectrophotometrically by measuring the activity of both the suspension and supernatant. To slow down the immobilization process of NOX on agarose, 10 mM hydroxylamine was added to the suspension. In the case of immobilization on methacrylate, 10 mM hydroxylamine and 154 mM ethanol were added to slow down the immobilization.

**PEI-Coating of NOX Immobilized on Agarose and Methacrylate Carriers.** When PEI-coating was applied after enzyme immobilization, 1 g of AG-G was mixed with 10 mL of a 10 mg/mL PEI solution in 100 mM bicarbonate buffer solution at pH 10 under orbital shaking for 1 h at 25 °C. Later on, solid NaBH<sub>4</sub> was added (final concentration of 1 mg/mL) and incubated for 30 min at 4 °C. Finally, AG-G/PEI25 was washed five times with 10 volumes of water and stored at 4 °C.

**Cofactor Co-immobilization.** After PEI coating, ionic adsorption of NADH was achieved by incubating 10 mL of 1 mM NADH solution in 10 mM sodium phosphate at pH 7 with 1 g of agarose microbeads with previously immobilized enzymes. The suspension was kept under orbital shaking for 1 h at room temperature. Afterward, the resin was filtered and washed three times with 1 mL of 10 mM sodium phosphate at pH 7. The immobilization yield of NADH was calculated by measuring the absorbance of the supernatant after the adsorption process and after each washing step at 340 nm in the well-plate reader.<sup>43</sup>

**NOX Activity through Monitoring H<sub>2</sub>O<sub>2</sub> Production.** 200 μL of reaction mixture containing 0.2 mM NADH, 0.15 mM FAD, 0.05 mM Ampliflu Red, and 25 μg/mL HRP in 25 mM sodium phosphate buffer at pH 7 was added to the immobilized biocatalyst. NOX immobilized on agarose (1 mg/g), the same biocatalyst coated with PEI, and another preparation coated with PEI and with co-immobilized NADH were used as immobilized biocatalysts. NADH and H<sub>2</sub>O<sub>2</sub> production were simultaneously monitored at 340 and 520 nm, respectively, at 25 °C for 15 min in the well-plate reader.

**Intraparticle Protein Distribution Analysis by Fluorescence CLSM.** 20 mg of the immobilized biocatalysts was added to 200 μL of buffer solution in an 8-well microslide. In the case of the methacrylate carrier, the buffer solution contained 50% glycerol to improve the match in the refractive index between the medium and the opaque beads. Since the intrinsic FAD of the enzyme exhibits autofluorescence, the spatial distribution of the enzyme across the carrier was analyzed using a ZEISS confocal microscope LSM880 with λ<sub>ex</sub> = 488 nm and λ<sub>ex</sub> = 520 nm. Images were processed with the software FIJI using a LUT (Yellow hot).

**Optochemical O<sub>2</sub> Sensing in Bulk Solution and inside the Solid Support.** The O<sub>2</sub> concentration in bulk solution was measured using a fiber optic oxygen microoptode (Optical Oxygen Meter –

FireStingO<sub>2</sub>). 100  $\mu$ L of a suspension of 1:10 (w/v) immobilized NOX on PU-G (0.1, 0.5, 1, and 3 mg/g) was added to 4 mL of substrate solution containing NADH (0.2, 1, 1.25, and 3 mM) and 0.025 mM FAD in air-saturated 25 mM sodium phosphate buffer at pH 7 in an open glass vial (1.2 cm diameter). The setup took place at 25 °C and 300 rpm magnetic stirring (6  $\times$  3 mm) as described before.<sup>4,5</sup> For the intraparticle O<sub>2</sub> sensing, two immobilized biocatalysts on PU-G with different protein loadings (0.1 and 3 mg/g) were labeled with Ru(dpp)<sub>3</sub> (25% of 5 g/L Ru(dpp)<sub>3</sub> in ethanol) in air-saturated 25 mM sodium phosphate buffer pH 7 at 30 °C. The Ru(dpp)<sub>3</sub> load was 5 mg/g. The suspension was incubated for 10 min at room temperature under orbital shaking. The excess Ru(dpp)<sub>3</sub> was washed out with the same buffer till the supernatant was clear. 200  $\mu$ L of a suspension of 1:10 (w/v) immobilized NOX was added to 4 mL of a substrate solution containing NADH (0.2 mM and 3 mM) and 0.025 mM FAD in air-saturated 25 mM sodium phosphate buffer at pH 7. The oxygen consumption was monitored as described elsewhere<sup>4</sup> (see supporting methodology in the Supporting Information for more details).

## ■ ASSOCIATED CONTENT

### SI Supporting Information

The Supporting Information is available free of charge at <https://pubs.acs.org/doi/10.1021/acsami.0c17568>.

Supporting methodology; influence of protein loading, mixing method, and enzyme distribution on the performance of the immobilized biocatalyst (Figures S1–S3); Langmuir isotherms for the ionic adsorption of NADH to different beads coated with PEI (Figure S4); CLSM micrographs for the immobilization of FAD and NAD<sup>+</sup> (Figures S5–S8); Michaelis–Menten plots of NOX immobilized with and without PEI and the effect of the cofactor co-immobilization on the activity of the immobilized NOX (Figures S9 and S10); and expression and purification of NOX (Figures S11) (PDF)

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### Author Contributions

Experiments were performed by ABM and CH. The manuscript was written by J.M.B. and F.L.G. The work was conceptualized by J.M.B. and F.L.G. Funding was secured by B.N., J.M.B., and F.L.G. All authors discussed the results and revised the manuscript. All authors have given approval to the final version of the present manuscript.

### Notes

The authors declare no competing financial interest.

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## ■ ABBREVIATIONS

AG-G, agarose microbeads activated with glyoxyl groups  
AG-G/PEI25, agarose microbeads activated with glyoxyl groups and coated with polyethyleneimine 25 kDa  
CLSM, confocal laser scanning microscopy  
FAD, flavin adenine dinucleotide  
HRP, peroxidase from horseradish  
IPTG, isopropyl- $\beta$ -D-1-thiogalactopyranoside  
 $K_d$ , dissociation constant  
LUT, look-up table for color grading  
NAD(H), nicotinamide adenine dinucleotide  
NADP(H), nicotinamide adenine dinucleotide phosphate  
NOX, NAD(P)H flavin oxidases  
PEI, polyethyleneimine  
PU-G, PuroLite ECR8215F (methacrylate) microbeads activated with glyoxyl groups  
ROI, region of interest

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